

Available Online at http://www.journalajst.com

ASIAN JOURNAL OF SCIENCE AND TECHNOLOGY

Asian Journal of Science and Technology Vol. 07, Issue, 09, pp.3602-3608, September, 2016

RESEARCH ARTICLE

SKIN IMPEDANCE AND MYOMETRY (ENF AND MYOTON): TWO INSTRUMENTS COMPARED IN ACUTE AND CHRONIC SOMATIC DYSFUNCTION

¹Bellomo, R.G., ^{2, *}Barassi, G., 2Giannuzzo, G., ²Di Felice, P.A., ³Porto, D. and ⁴Saggini, R.

¹Department of Medicine and Science of Aging, "G.d'Annunzio" University, Chieti-Italy ²Faculty of Physiotherapy "G.d'Annunzio" University, Chieti-Italy ³School of Specialties in PRM, "G.d'Annun zio" University, Chieti- Italy ⁴Department of Medical Sciences, Oral and Biotechnology, "G.d'Annunzio" University, Chieti-Italy

| ARTICLE INFO | ABSTRACT |
|--|--|
| Article History: Received 14 th June, 2016 Received in revised form 16 th July, 2016 Accepted 28 th August, 2016 Published online 30 th September, 2016 | In rehabilitation medicine can be observed tissue alterations that go to join in specific disease states, and may be the first signal to decode a dysfunctional state and program the rehabilitation protocol. Somatic dysfunction present alternations of tone and tissue quality, the perception of pain at specific points during the evaluation, anatomical asymmetries and reductions in the ROM. The purpose of this study was to compare in a single-bind dysfunctional areas previously identified with a clinical functional assessment studied through the use of two different devices: the ENF, an impedance evaluation system |
| Key words: | that measures the rheological skin values and the Myoton, which measures the elasticity, deformability and the tone of the tissue district with a scientifically validated system. The results were able to show |
| Somatic dysfunction, Interactive neuromodulation, Myometry, Patient assessment. | all the typical neurophysiological characteristics related to somatic dysfunction, considering concepts such as facilitation, neurogenic inflammation, up to the concept of allostatic overload, the final result of the stress accumulated sum and daily dysfunction during various activities of everyday life. |

Copyright©2016, Akpan et al. This is an open access article distributed under the Creative Commons Attribution License, which permits unrestricted use, distribution, and reproduction in any medium, provided the original work is properly cited.

INTRODUCTION

In rehabilitative medicine results important consider that the tissue alterations are mediated by diseases and autonomic reactions (Budgell et al., 1998). Whatever the pain areas, often primary dysfunction becomes the first signal to decode before design and applying a rehabilitation protocol. The efferent somatic areas are often the clearest demonstration of how at spinal cord level subcortical and cortical informational alterations and the specific disease, could change myofascial tissue peripherally (Kimura, 1997; Sato, 1997). Therefore, the clinician needs to understand and manage this condition of suffering to be able to interpret somatic dysfunction and treat it in a properly physiological modality. Myofascial dysfunction, expression of many pathological conditions, can be objectified through the use of myoton and supported by the operator's functional evaluation (Kagitani et al., 1996). The interpretation of the somatic dysfunction is equivalent to objectify increased discharge of "gamma motor neurons" to intrafusal fibers of the muscle spindle to "increase profits" of spindles which produce a prolonged reflex muscle contraction

*Corresponding author: Barassi, G.,

Department of Medicine and Science of Aging, "Gabriele d'Annunzio" University, Chieti-Italy.

("neurological muscle tone") (Cervero, 2009). The segmental muscle contraction should produce a tissue modification and restriction of the joint segmental movement, even in apparently healthy, asymptomatic subjects. The clinical evidence of somatic dysfunction includes: alteration of the tissue quality or the soft tissue tone, the perception of pain in the points identified during the evaluation, the anatomical asymmetries, the range of motion alteration (Korr, 1975). Aim of this controlled randomized single-blind study is to compare the dysfunctional areas, found in clinical and functional assessment performed by the clinician and an impedance evaluation system that focuses on rheological values and skin impedance, with a tissue evaluation system already scientifically validated, the myoton. Examining the tone, biomechanical and viscoelastic properties of skeletal muscles is proposed a complementary, non-invasive and cost-effective technology that enables real-time assessment of muscles (Chuang et al., 2013). Changes in muscle tone and properties could be used to assess effects of pathology (Dahmane et al., 2001), sport-related injury or therapeutic intervention (Ratsep, 2011). Such assessments could be performed at regular intervals to monitor the stage of the pathological processes of muscles and for assessing efficacy of therapeutic interventions (Marusiak et al., 2012).

The measurement method applied in the Myoton Pro is based on exertion of a quick released single mechanical impulse (time 15 ms, force 0.4 N) under constant pre-compression force (0.18 N) of the subcutaneous tissue layer above the muscle/tendon being measured. Mechanical deformation is delivered by the device testing end (d = 3 mm), held perpendicular to the skin surface. After a short mechanical impulse, the muscle or tendon responds in the form of a damped oscillation, which is registered by an acceleration sensor attached to the device's frictionless measuring mechanism. The properties of the sensor are as follows: amplitude range of ± 8 g in full range; resolution of <0.001 g; output data rate and bandwidth 3,200 Hz; sensitivity of <20 mg/LSB for each axis; sensitivity ± 0.1 % due to the temperature change; bias level of each axis 100 mg; noise performance of each <1.5 LSB rms; and operating temperature -10 to +50C. While stiffness, tone and elasticity are the most commonly reported parameters using Myoton devices in the literature (Aird et al., 2012), We additionally investigated mechanical stress relaxation time and indication of creep in the present study to document the behaviour of all five parameters and relative changes to one another under the known influence of unloading in weightlessness. The target wants to be find a match of interpretive values of the dysfunction, among the areas identified by the operator using specific tests, with greater reduction of ROM, greater tissue alteration (using rolling test), rheological values recorded with the myoton and values of skin impedance recorded with ENF technology. ENF (Electro neurofeedback) is a tool with the ability to communicate with the body with a frequency of at least 90 times per second. It can be defined Interactive Neuroregolator for its both evaluative and rehabilitative ability. It is able to read the impedance values of the skin and to transmit electrical impulses through a special algorithm for interact with the organism.

The interactive neuromodulation is a form of electrotherapy characterized by:

- Biphasic damped sinusoidal signal variable in time, with morphological characteristics similar to ECG
- Potential of action of high amplitude, short and not harmful
- Absence of the adaptation process thanks to the feedback that always generates different signals depending on the skin impedance alterations.

Two different phases of employment are distinghuished:

- The enf identifies the area that needs treatment, it does not necessarily correspond with algic area
- The therapeutic modality is adopted by the ENF (Electro Neuro Feedback) based on the reading of the level of the skin's impedance, at the same time sends a stimulus using an algorithm that interacts with SNC.

The stimuli are represented by bipolar and biphasic electrical pulses at very low frequencies from 15 to 350 Hz. At the basis of the action of this electrotherapy and in particular of ENF, there is the interactive mechanism neuroregulation that allows the patient to obtain a dynamic balance of the organism in relation with the environment to reach the 'homeostasis and therefore the health state.

The adjustment of all the vital functions is realized through a strict connection and interaction of the endocrine and nervous systems, which effects are mediated through the release by neural cells of biologically active substances called neuromediators (NM); amines (acetylcholine, norepinephrine, etc.) and amino acids (glutamine, asparagin, etc.), characteristics elements of fibers A-Beta, myelinated nerve neurotransmitters fibers are classic (acetylcholine, norepinephrine, etc.) and have a well-defined physiological fast and short effect; neuropeptides (NP) that are, from a physiological and medical point of view, the biggest and most important group of neuromodulators include: endorphins, enkephalins, neurotensine, bradykinin, and a large number of other types (more than 2000 in total); These are principal neuromodulators for thin and not myelinated and particularly difficult to stimulate C fibers. These neuropeptides are produced from fibers which constitute the majority (over 70%) of the nervous pathways. Science has already shown that because of their long-term specific properties and action away from the site of production, are responsible for the formation of complex regulative chains and of drops for the control of various physiological functions, in addition to the potent analgesic effect, etc. (Laird et al., 2001; Cervero, 2000). Precisely for this reason that the target tissue of the action of ENF is represented mainly by nervous tissue; Its stimulation allows to obtain results because it activates the production of an effective dose of neuropeptides, released by the stimulation of C-fibers and necessary to overcome the existing alteration of human body.

MATERIALS AND METHODS

The research protocol is compatible with the Declaration of Helsinki; as part of the Chair of Physical and Rehabilitation Medicine, University of Chieti, they were selected 20 patients (10 males 10 females), who had been diagnosed with a trigger points myofascial syndrome.

Inclusion criteria:

- Myofascial syndrome involving the trapezius muscles, minor pectorals, rhomboids, quadratus lomborum, quadriceps
- Algic syndrome involving the neck region
- Algic syndrome involving gleno-humeral joint
- Algic syndrome involving lumbar region
- Algic syndrome involving knee joint
- Age beetwen 18 and 40 years old

Exclusion Criteria

- Radicular syndrome diagnosis
- Dismetabolic disease
- Pharmacologic treatments in progress

The subjects have been subjected to a global postural clinical evaluation, divided into three phases:

- Functional and structural evaluation: to identify any limitations, asymmetries and tissue dysfunction
- Muscular evaluation, by Myoton, into the areas previously identified as dysfunctional, with altered

values of ROM and tissue quality (by rolling test) assessed by the clinician

• Tissue evaluation with enf: areas resulted dysfunctional in the tests, together with contralateral areas, are subjected to impedeziometric evaluation.

In the areas identified with the clinician's functional assessment is performed the muscluar evaluation using Myoton that will provide datas of three parameters:

- Frequency: muscular elasticity
- Decrement: musucar tone
- Stiffness: muscular rigidity

Oscillation Frequency [Hz]

Indicates the Tone (that is, intrinsic tension) of a muscle in its passive or resting state without any voluntary contraction (EMG base level). Hypertonia and respectively increased intramuscular pressure causes reduced blood supply, which brings on worse muscle recovery and quicker muscle fatigue. Oscillation Frequency in contracted state indicates the tension of a muscle.

Logarithmic Decrement - no unit of a muscle's natural oscillation indicates the muscle's elasticity. Elasticity is the biomechanical property of a muscle that characterises the ability to recover its initial shape after a contraction or removal of an external force. Elasticity is inversely proportional to the decrement. Decrement describes the dissipation of mechanical energy in the tissue during one oscillation cycle. If the muscle dissipates less mechanical energy then it is more elastic. If the muscle is more elastic then it is more economic and efficient in function. The inverse of Elasticity is Plasticity.

Dynamic Stiffness [N/m]

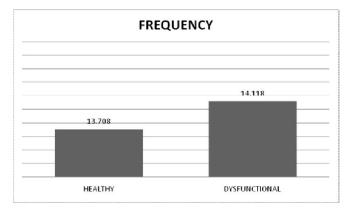
Stiffness is the biomechanical property of a muscle that characterises the resistance to a contraction or to an external force that deforms its initial shape. Greater effort is required from the agonist muscle to extend the antagonist muscle with high stiffness, which leads to inefficient economy of movement. The term Dynamic Stiffness originates from the dynamic measurement method applied in Myoton PRO. The inverse of Stiffness is Compliance. The stages to use of interactive neurostimulator ENF are two:

- The ENF identifies the area that needs treatment not corresponding with algic area
- The evaluation mode is implemented by ENF based on the reading of the skin impedance level and simultaneously is achieved a stimulus using a specific algorithm that interacts with the SNC through the interaction with the skin organ.

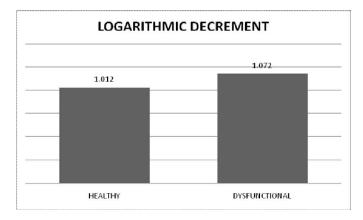
The stimuli are represented by bipolar and biphasic electrical pulses at very low frequencies from 15 to 350 Hz. Relying on his special pulse generation algorithm, the ENF modifies the output signal based on the neurological response projected on the skin. This process causes a skin reaction very quickly, easily making a first diagnostic indication on where an anomaly is manifested by the body. The first phase of ENF is called manual scan. To scan manually, the electrode is placed on the skin and the instrument is moved making a dynamic action (painting) on the area to be evaluated. The dynamic action should be repeated in four directions as to form a cross, keeping the electrode well placed while scrolling. After a few moments (typically a few seconds) they will appear some changes in the skin that we will call reactive zones, which manifest themselves with a reddening and an impedance change. The ENF digitally scan mode uses an algorythm to generate a pulse, varying the signal according to the neurological response of the skin. This process causes a skin reaction very quickly, easily forming a first diagnostic indication on where an anomaly is manifested by the body.

RESULTS

Are shown below tables and graphs are related to the assessments made with Myoton and ENF on the examined sample. From these assessments we can confirm that after the evaluation of the patient with specifical physical and clinical tests, having identified the dysfunctional area, we can corroborate the result of the functional evaluation with a second assessment by the use of ENF and myoton making a measurement of the rheological values and impedance of skin tissue. This valuations, that are not operator-linked, have confirmed the topographic location of the dysfunctional area. From the analysis of the obtained data, we separate the two groups, depending on whether it were a chronic or acute dysfunction.



Graphic n°1. The graph shows the average values of the frequency, i.e. muscle tension, greater in the dysfunctional side than the healthy one by a value of 0.41 points



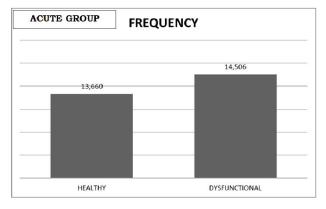
Graphic n°2. the graph shows the average values of the Logarithmic Decrement, i.e. muscle elasticity, greater in the dysfunctional side of 0.06 points compared to the healthy one

| Patient | | Myoton | | | Enf | Note | |
|---------|-----|---------------|-------|------|-----|------|--------------------------|
| | | - | F | D | S | FR | |
| Chronic | P 1 | Healthy | 11,06 | 0,98 | 117 | 15 | Left upper trapezius |
| | | Disfunctional | 10,2 | 1,01 | 113 | 16 | |
| Acute | P2 | Healhty | 13,5 | 0,89 | 233 | 31 | Right quadricep |
| | | Disfunctional | 14,16 | 1,01 | 261 | 88 | U |
| Acute | P3 | Healthy | 10,6 | 1,2 | 125 | 40 | Right upper trapezius |
| | | Disfunctional | 11,6 | 1,28 | 158 | 79 | 0 11 1 |
| Acute | P4 | Healthy | 13,7 | 0,92 | 216 | 39 | Right quadratus lumborum |
| | | Disfunctional | 16,1 | 1,03 | 327 | 84 | 0 |
| Chronic | P5 | Healthy | 12,6 | 0,94 | 193 | 12 | Left quadratus lumborum |
| | | Disfunctional | 12,2 | 0,88 | 176 | 8 | • |
| Chronic | P6 | Healthy | 15,2 | 1,09 | 258 | 12 | Left upper trapezius |
| | | Disfunctional | 14,5 | 0,96 | 235 | 6 | 11 1 |
| Chronic | P7 | Healthy | 11.8 | 0,7 | 140 | 8 | Right tibialis anterior |
| | | Disfunctional | 11,5 | 0,61 | 122 | 6 | 5 |
| Acute | P8 | Healhty | 11 | 0,96 | 125 | 63 | Right minor pectoral |
| | | Disfunctional | 10,7 | 1,33 | 161 | 97 | <i>c</i> 1 |
| Chronic | P9 | Healthy | 18,6 | 1,19 | 360 | 13 | Left upper trapezius |
| | | Disfunctional | 17,3 | 1 | 315 | 9 | |
| Chronic | P10 | Healthy | 9,9 | 1,02 | 132 | 10 | Right quadratus lomborum |
| | | Disfunctional | 10 | 1,16 | 133 | 6 | 0 1 |
| Chronic | P11 | Healthy | 14,6 | 1,35 | 254 | 10 | Left minor pectoral |
| | | Disfunctional | 15,7 | 1,56 | 279 | 8 | 1 |
| Acute | P12 | Healhty | 13,5 | 0,69 | 183 | 44 | Left upper trapezius |
| | | Disfunctional | 15,9 | 0,7 | 249 | 94 | |
| Chronic | P13 | Healthy | 13,8 | 1,16 | 198 | 14 | Right quadricep |
| | | Disfunctional | 12,9 | 1,28 | 186 | 8 | |
| Acute | P14 | Healhty | 12,7 | 0,88 | 204 | 45 | Left tibialis anterior |
| | | Disfunctional | 12,3 | 0,78 | 170 | 67 | |
| Acute | P15 | Healhty | 13,2 | 0,76 | 165 | 45 | Left quadratus lomborum |
| | | Disfunctional | 12,7 | 0,68 | 152 | 78 | 1 |
| Acute | P16 | Healhty | 17,3 | 1,12 | 326 | 29 | Right lat |
| | | Disfunctional | 17,3 | 1,31 | 335 | 73 | U |
| Acute | P17 | Healhty | 18 | 1,08 | 372 | 37 | Left lat |
| | | Disfunctional | 18,1 | 1,18 | 377 | 69 | |
| Chronic | P18 | Healthy | 16,3 | 1,2 | 369 | 8 | Right medium trapezius |
| | | Disfunctional | 16,8 | 1,26 | 353 | 6 | 5 P |
| Chronic | P19 | Healthy | 13,7 | 0,99 | 203 | 11 | Left upper trapezius |
| | | Disfunctional | 16,2 | 0,94 | 394 | 7 | |
| Acute | P20 | Healhty | 13,1 | 1,12 | 227 | 37 | Right minor pectoral |
| | | Disfunctional | 16,2 | 1,48 | 298 | 79 | 0 · · · · · · |

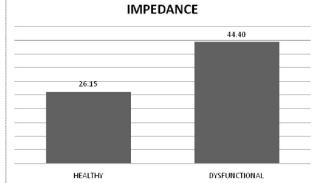


Graphic 3. The graph shows the average values of Stiffness, ie the stiffness, greater in the dysfunctional side of 19.7 points compared to the healthy one

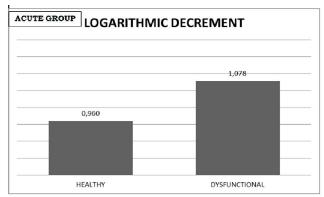
Acute group



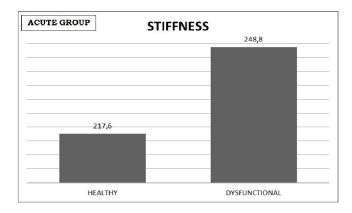
ie muscle tension, greater in the dysfunctional side of 0.85 points compared to healthy subjects with acute dysfunction



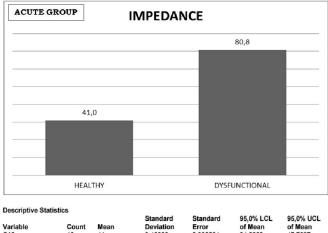
Graphic 4. The chart shows the average values of skin impedance, recorded through the use of ENF, greater in the dysfunctional side of 18.25 points compared to the healthy side



Graphic 5. The graph shows the average values of the frequency, Graphic 6. The graph shows the average values of the Logarithmic Decrement, ie the muscle elasticity, increased by 0.2 points in the dysfunctional side compared to healthy subjects with acute dysfunction



Graphic 7. The graph shows the average values of Stiffness, i.e. the stiffness, greater in the dysfunctional side of 31.2 points compared to healthy subjects with acute dysfunction



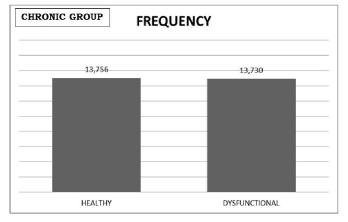
| Variable | Count | Mean | Deviation | Standard | 95,0% LCL of Mean | 95,0% UCL of Mean |
|------------------|------------------|---------------|-------------------|----------|----------------------|----------------------|
| C12 | 10 | 41 | 9,46338 | 2,992584 | 34,2303 | 47,7697 |
| C16 | 10 | 80,8 | 10,01998 | 3,168596 | 73,63214 | 87,96786 |
| T* for Confident | ce Limits: T* (C | 12) = 2,2622; | T* (C16) = 2,2622 | | | |

Two-Sided Confidence Interval of the Mean Difference

| | | | | | | | 95,0% C. I. | or mean Diff. |
|---|----------------------------|-----------------------------|-----------------------------------|-------------------------------|----------------------|-------------------------|-----------------------------|-----------------------------|
| Variables C12 - C16 | Count 10 | Mean Difference -39,8 | Standard Deviation 10,04213 | Standard Error 3,175601 | T * 2,2622 | d.f. 9 | Lower Limit -46,98371 | Upper Limit -32,61629 |
| Paired-Sample Paired Difference | | 16) | | | | | | |
| Alternative Hypothesis Mean Diff. ≠ 0 | Mean Differend -39,8 | Standa Error 3,1756 | т-8 | tatistic 5331 | d.f . 9 | Prob Level 0,0000 | at a | ct H0 = 0,050 |

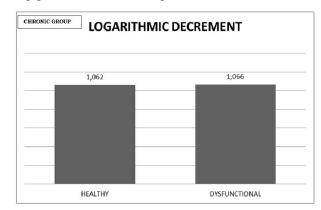
05.0% C L of Moon Diff

Graphic 8. The chart shows the average values of skin impedance, greater in the dysfunctional side of 39.8 points compared to healthy subjects with acute dysfunction

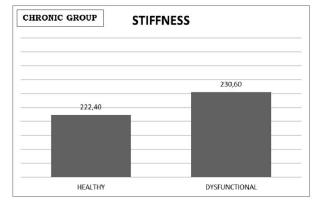


Graphic 9. The graph shows the average values of the frequency, ie muscle tension, greater in the dysfunctional side compared to healthy subjects with chronic dysfunction

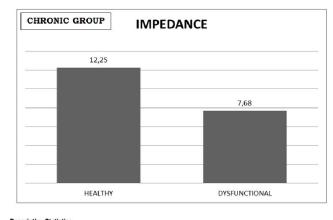
Group patients with chronic pain



Graphic 10. The graph shows the average values of the Logarithmic Decrement, ie the muscle elasticity, greater in the dysfunctional side 0,004 points compared to healthy subjects with chronic dysfunction



Graphic 11. The graph shows the average values of Stiffness, ie the stiffness, greater in the dysfunctional side of 8.2 points compared to healthy subjects with chronic dysfunction



| 2017-21 Mol - 98 99-802200 125 | | | Standard | Standard | 95,0% LCL | 95,0% UCL |
|--------------------------------|------------------|--------------|------------------|-----------|-----------|-----------|
| Variable | Count | Mean | Deviation | Error | of Mean | of Mean |
| C4 | 10 | 11,3 | 2,359378 | 0,746101 | 9,612203 | 12,9878 |
| C8 | 10 | 8 | 3,018462 | 0,9545214 | 5,840723 | 10,15928 |
| T* for Confiden | ce Limits: T* (C | 4) = 2,2622; | T* (C8) = 2,2622 | | | |

Two-Sided Confidence Interval of the Mean Difference

| | | | | | | | | of Mean Diff. |
|------------------------------------|-----------|--------------------|-----------------------|-------------------|--------|---------|----------------|----------------|
| Variables | Count | Mean Difference | Standard Deviation | Standard Error | T* | d.f. | Lower Limit | Upper Limit |
| C4 - C8 | 10 | 3,3 | 2,110819 | 0,6674995 | 2,2622 | 9 | 1,790011 | 4,809988 |
| Paired-Sample Paired Difference | |) | | | | | | |
| Alternative | Mean | Standa | ard | | | Prob | Reje | ct H0 |
| Hypothesis | Differend | ce Error | т-5 | Statistic | d.f. | Level | at a | = 0,050 |
| Mean Diff. ≠ 0 | 3.3 | 0.6674 | 995 4.9 | 438 | 9 | 0.00080 |) Yes | |

Graphic 12. The graph shows the average values of skin impedance, greater in the dysfunctional side of 4.57 points compared to healthy subjects with chronic dysfunction

In case of chronic dysfunction, the skin impedance values, measured with ENF, resulted low, while in case of acute dysfunction such values resulted to be high.

DISCUSSION AND CONCLUSION

The conducted study showed all the neurophysiological characteristics of somatic dysfunction, considering notions such as facilitation, neurogenic inflammation, until reaching definitions as "allostatic overload", true final result of the amount of stresses and the dysfunctions accumulated during daily activities. This condition must be eliminated in order to restore the health status of the patient (Cervero and Laird, 1996). The assessment is therefore an important and crucial time to plan an effective and causal intervention (Korr et al., 1964). The effect of skin temperature and hydration status has been suggested by some researchers as a common cause of variation in bioimpedance measurements of the body (Podtaev et al., 2015; Cornish et al., 1998). This paper details a simple method of measuring the impedance of the skin, in somatic dysfunction (Thomas and Korr, 1951). The functional evaluation, operator-dependent, have been joined by two objective evaluations (Myoton-myometry- and ENF- skin impedance).

The ENF confirmed the neurophysiological and mechanic interconnection concepts of the somatic tissue with the afferent receptorial system, which is capable of synergistically express an efferent manifestation at all these levels. From the data collected we can see that the characteristics of the tissues showed different results in instrumental and even manual assessments by the operator. The tools used validate the importance of a clear identification of the dysfunctinal area needing treatment. Pressure, cleaning the skin with alcohol, and exfoliation did not affect the performance of the ENF device. Our new device has some properties which can make it a good choice for future researches. It connects and records electrical skin impedance of each probe automatically. This device has one probe and is able to connect to different locations at the same time. This can happen because most of the sensory, somatic motory and visceral nerves show a clear anatomical and functional arrangement of metameric type in their course towards and from the spinal cord and since the centers of the vertebral reflections are capable of coordinating and modeling the interchange of somatic and visceral reflex even in the complete absence of supraspinal reflex centers (Korr, 1951). It can also be used for a prolong period in recording electrical skin impedance, and for therapeutic use through specific programs (not used in this research work).

Conflict of interest

All authors declare that there is no personal interest properties, financial, professional or other of any nature or kind in any product, service or company that could be interpreted as influencing the position presented in this manuscript.

REFERENCES

Aird, L., Samuel, D., Stokes, M. 2012. Quadriceps muscle tone, elasticity and stiffness in older males: reliability and symmetry using the MyotonPRO., Arch Gerontol Geriatr, 55(2):e31-e39-.

- Budgell, B.S., Hotta, H., Sato, A. 1998. Reflex_responses of bladder motility after stimulation of interspinous tissues in the anesthetized rat., *J Manipulative Physiol Ther.*, Nov-Dec;21(9):593-9
- Cervero F, Laird JM. 1996. Mechanisms of touch-evoked pain (allodynia): a new model, *Pain*, Nov;68(1):13-23. Review
- Cervero F. 2000. Visceral pain-central sensitisation, *Gut*, Dec;47 Suppl 4:iv56-7; discussion iv58. Review
- Cervero, F. 2009. Spinal cord hyperexcitability and its role in pain and hyperalgesia, *Exp Brain Res.*, Jun; 196(1):129-37. doi: 10.1007/s00221-009-1789-2. Epub 2009 Apr 7. Review
- Chuang, L.L., Lin, K.C., Wu, C.Y., Chang, C.W., Chen, H.C., Yin, H.P., Wang, L. 2013. Reliabilities of relative and absolute measurements get by Myoton, are tested on hemiparetic arms in patients with stroke, *Arch Phys Med Rehabil*, 94(3):459–466
- Cornish, B.H., Thomas, B.J., Ward, L.C. 1998. Effect of temperature and sweating on bioimpedance measurements, *Appl Radiat Isot*, 1998 May-Jun; 49(5-6):475-6.
- Dahmane, R., Valeni, V., Knez, N., Eren, I. 2001. Evaluation of muscle contractile properties, on the basis of the muscle belly response, through non-invasive estimation of the muscle belly response, *Med Biol Eng Comput*, 39(1):51–55
- Kagitani, F., Kimura, A., Sato, A., Suzuki, A. 1996. The role of the spinal cord as a reflex_center for the somatically induced_reflex_responses of splenic sympathetic and natural killer cell activity in anesthetized rats, *Neurosci Lett.*, Oct 18;217(2-3):109-12
- Kimura, A., Sato, A. 1997. Somatic_regulation of autonomic functions in anesthetized animals--neural mechanisms of physical therapy including acupuncture, *Jpn J Vet Res.*, Nov;45(3):137-45. Review.
- Korr Im, Wright Hm, Chace Ja. (1964) Cutaneous Patterns Of Sympathetic Activity In Clinical Abnormalities Of The Musculoskeletal System, *Acta Neuroveg*, (Wien) ;25:589-606
- Korr, I.M. 1951. The somatic approach to the disease process, J Am Osteopath Assoc, Dec; 51(4):201-5
- Korr, I.M. 1975. Proprioceptors and somatic dysfunction, *J Am Osteopath Assoc.*, Mar; 74(7):638-50. Review
- Laird, J.M., Roza, C., De Felipe, C, Hunt SP, Cervero F. 2001. Role of central and peripheral tachykinin NK1 receptors in capsaicin-induced pain and hyperalgesia in mice, *Pain*, Feb 1;90(1-2):97-103
- Marusiak, J., Jaskolska, A., Koszewicz, M., Budrewicz, S., Jaskolski, A. 2012. Myometry revealed medicationinduced decrease in resting skeletal muscle stiffness in Parkinson's disease patients, *Clin Biomech* (Bristol, Avon) 27(6):632–635
- Podtaev S, Nikolaev D, Samartsev V, Gavrilov V, Tsiberkin K 2015. Frequency and temperature dependence of skin bioimpedance during a contralateral cold test, *Physiol Meas*, Mar; 36(3):561-77. doi: 10.1088/0967-3334/36/3/561. Epub 2015 Feb 18.
- Ratsep, T., Asser, T. 2011. Changes in viscoelastic properties of skeletal muscles induced by subthalamic stimulation in patients with Parkinson's disease. *Clin Biomech*, (Bristol, Avon) 26(2):213–217

Sato, A. 1997. Neural mechanisms of autonomic responses elicited by somatic sensory stimulation, *Neurosci Behav Physiol.*, Sep-Oct; 27(5):610-21. Review Thomas, P.E, Korr, I.M. 1951. The automatic recording of electrical skin resistance patterns on the human trunk,